

Generative AI Mitigates Representation Bias Using Synthetic Health Data

Nicolo Micheletti^{1,2†}, Raffaele Marchesi^{2,5†}, Nicholas I-Hsien Kuo³, Sebastiano Barbieri³, Giuseppe Jurman² and Venet Osmani⁴

¹Department of Computer Science, University of Manchester, United Kingdom.

²Fondazione Bruno Kessler Research Institute, Italy.

³Centre for Big Data Research in Health, University of New South Wales, Australia.

⁴Information School, University of Sheffield, United Kingdom.

⁵University of Pavia, Italy.

Contributing authors: nicolo.micheletti@student.manchester.ac.uk; rmarchesi@fbk.eu; n.kuo@unsw.edu.au; s.barbieri@unsw.edu.au; giuseppe.jurman@fbk.eu; v.osmani@sheffield.ac.uk;

[†]These authors contributed equally to this work.

Abstract

Representation bias in health data can lead to unfair decisions, compromising the generalisability of research findings. As a consequence, underrepresented subpopulations, such as those from specific gender or ethnic backgrounds do not benefit equally from clinical discoveries. Several approaches have been developed to mitigate representation bias, ranging from simple resampling methods, such as SMOTE, to recent approaches based on generative adversarial networks (GAN). However, generating high-dimensional time-series synthetic health data remains a significant challenge. In this work, we propose a novel CA-GAN architecture that synthesises authentic, high-dimensional time series data. CA-GAN outperforms state-of-the-art methods in a qualitative and a quantitative evaluation while avoiding mode collapse, a serious GAN failure. We evaluate our CA-GAN's generalisability in mitigating representation bias for Black patients, as well as female patients, in two diverse, clinically relevant datasets: acute hypotension and sepsis. Finally,

we show that CA-GAN generates authentic data of the minority class while faithfully maintaining the original distribution of both datasets.

Keywords: generative adversarial networks, synthetic data, resampling, oversampling, bias, underrepresentation, health data

1 Introduction

Clinical practice is poised to benefit from developments in machine learning as data-driven digital health technologies transform health care [1]. Digital health can catalyse the World Health Organisation’s (WHO) vision of promoting equitable, affordable, and universal access to health and care [2]. However, as machine learning methods increasingly weave themselves into the societal fabric, critical issues related to fairness and algorithmic bias in decision-making are coming to light. Algorithmic bias can originate from diverse sources, including socio-economic factors, where income disparities between ethno-racial groups are reflected in algorithms deciding which patients need care [3]. Bias can also originate from the underrepresentation of particular demographics, such as ethnicity, gender, and age in the datasets used to develop machine learning models, known as health data poverty [4]. Health data poverty impedes underrepresented subpopulations from benefiting from clinical discoveries, compromising the generalisability of research findings and leading to representation bias that can compound health disparities.

Machine learning community has developed several approaches to correct representation bias, with data resampling being the most widely used. Over-sampling generates representative synthetic data from the underrepresented subpopulation (minority class), resulting in a similar or equal representation. Synthetic Minority Over-sampling TEchnique (SMOTE) [5] is a representative example of this method, where synthetic samples lie between a randomly selected data sample and its randomly selected neighbour (using k-nearest neighbour algorithm [6]). SMOTE and related methods [7–9] are popular approaches due to their simplicity and computational efficiency.

However, SMOTE, when used with high-dimensional time-series data, may decrease data variability and introduce correlation between samples [10–12]. In response, alternative approaches based on Generative Adversarial Networks (GAN) are gaining ground [13–17]. GANs have shown incredible results in generating realistic images [18], text [19], and speech [20] in addition to improving privacy [21]. However, while GANs address some of the issues of SMOTE-based approaches, the generation of high-dimensional time-series data remains a significant research challenge [22–24].

To address this challenge, we propose a new generative architecture called Conditional Augmentation GAN (CA-GAN). Our CA-GAN extends Wasserstein GAN with Gradient Penalty [25, 26], presented in the Health Gym study

[27] (referred to in this paper as WGAN-GP*). However, our work has a different objective. Instead of generating new synthetic datasets, we condition our GAN to augment the minority class only while maintaining correlations between the variables and correlations over time. As a result, CA-GAN captures the distribution of the overall datasets, including the majority class. We compare the performance of our CA-GAN with WGAN-GP* and SMOTE in augmenting data of patients of an underrepresented ethnicity (Black patients in our case) as well as gender (female), using two critical care datasets of 7535 patients, comprising acute hypotension (n=3343) and sepsis (n=4192).

Our datasets include both categorical and continuous variables with diverse distributions and are derived from the well-studied MIMIC-III critical care database [28]. While these datasets were chosen as a proof of concept, our architecture is disease agnostic.

Our work makes the following contributions: (1) We propose a new CA-GAN architecture to mitigate representation bias, addressing the shortcomings of both, the traditional and the state-of-the-art methods in generating high-dimensional, time-series, synthetic data. (2) Our multi-metric evaluation using qualitative and quantitative methods demonstrates superior performance of CA-GAN with respect to the state of the art architecture, while avoiding a significant GAN failure, namely the mode collapse. (3) We also evaluate our CA-GAN against SMOTE, a naive but effective and popular resampling method, demonstrating the superior performance of generative models in the generalisation and synthesis of authentic data. (4) We show that CA-GAN can synthesise realistic data to augment the real data when used in a downstream predictive task. (5) We show the generalisability of CA-GAN in mitigating ethnicity and gender representation bias in two different but clinically relevant conditions, namely acute hypotension and sepsis.

2 Results

To evaluate the performance of our architecture, we compare the synthetic data generated by our CA-GAN with the data generated by state-of-the-art WGAN-GP* and SMOTE using a multi-metric evaluation.

Considering significant challenges in evaluating generative models in general, [29], and high-dimensional time-series data in particular, [23], we adopted a holistic approach to evaluating our work based on both qualitative and quantitative methods. We present the results of the data generated by the three methods to balance the original datasets, compared with the real patients of the minority class, namely Black ethnicity (shown in the main text) and female gender (shown in Appendix G).

2.1 Qualitative evaluation

To gain initial insights into the obtained results, we conduct a qualitative evaluation employing visual representation methods that show the coverage of synthetic data with respect to the real data. We use Principal Component

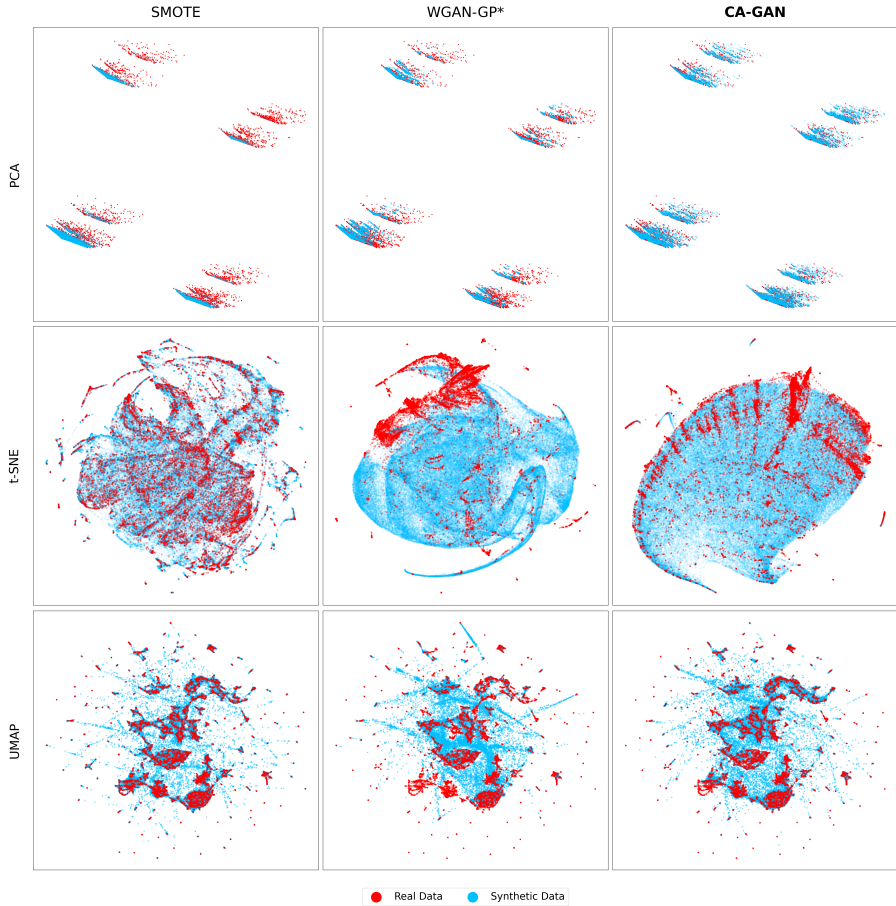
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Fig. 1: Two-dimensional representations of the acute hypotension dataset for Black patients. Top panels: PCA two-dimensional representation of real and synthetic data, where CA-GAN provides the best overall coverage of real data distribution, followed by SMOTE and WGAN-GP*, which shows evidence of mode collapse. Middle panels: t-SNE two-dimensional representation of real data (red) and synthetic data (blue) for the three methods SMOTE, WGAN-GP*, and CA-GAN. Bottom panels: UMAP two-dimensional representation, with the models having similar latent distributions.

Analysis (PCA) to project the real and synthetic data onto a two-dimensional space. We also use t-distributed Stochastic Neighbor Embedding (t-SNE) [30] to plot both real and synthetic datasets in a two-dimensional latent space while preserving the local neighbourhood relationships between data points. To note is that the stochastic nature of t-SNE results in differently shaped coverage graphs, while this is not the case for PCA. Lastly, we leverage Uniform Manifold Approximation and Projection (UMAP) [31], which offers better preservation of

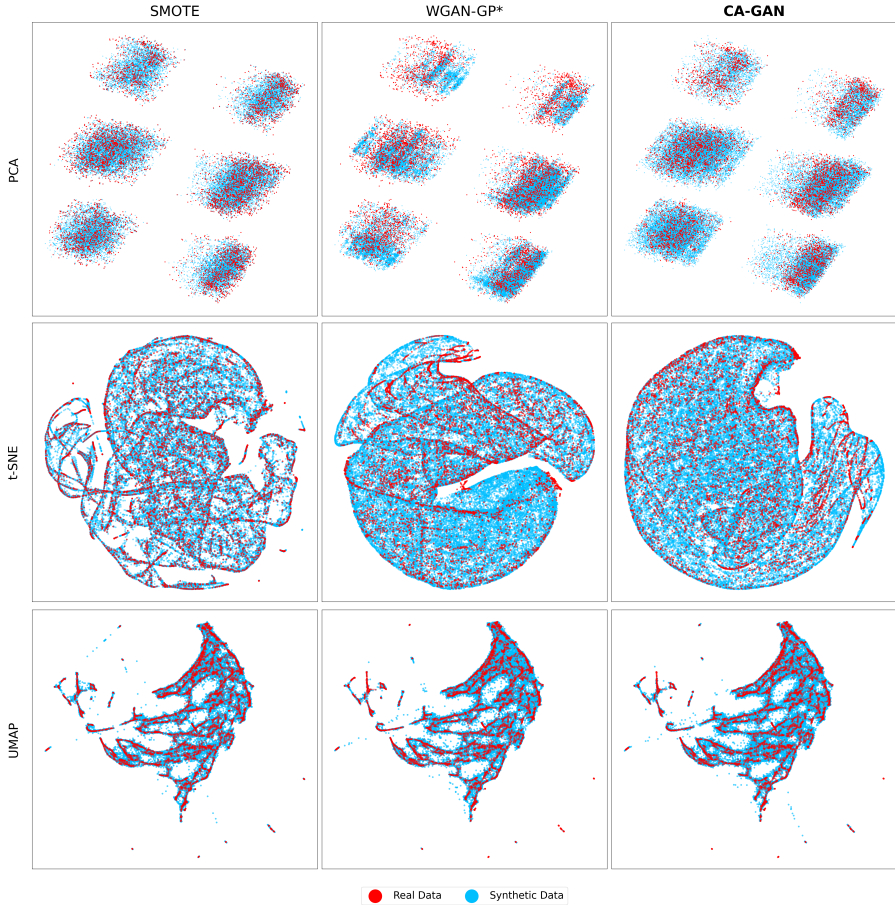


Fig. 2: Two-dimensional representations of the sepsis dataset for Black patients. Top panels: PCA two-dimensional representation of real and synthetic data, where CA-GAN provides the broadest coverage of the latent distribution, followed by SMOTE, while WGAN-GP* tends to converge. Middle panels: t-SNE two-dimensional representation of real data (red) and synthetic data (blue) for the three methods SMOTE, WGAN-GP*, and CA-GAN. It can be seen that the three methods provide different coverage of the latent distribution, with CA-GAN being the most homogeneous. Bottom panels: UMAP two-dimensional representation, where the three methods have the most similar distribution.

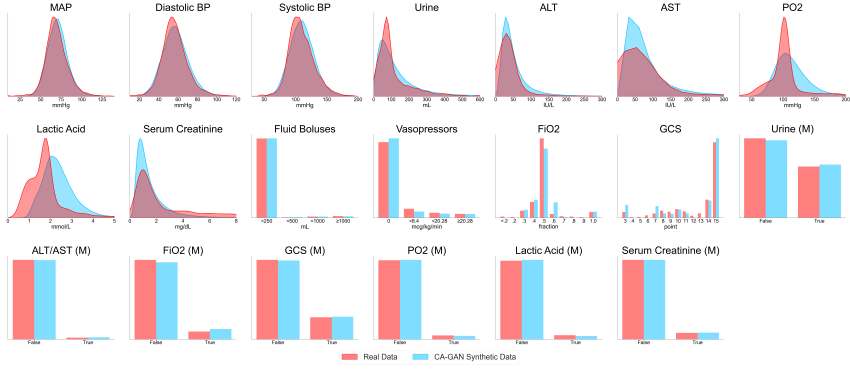
the global structure of the dataset when compared to t-SNE. The parameters of t-SNE and UMAP are the same for all three methods as shown in Appendix C).

The results of our representation are illustrated in the top panels of Figure 1 (acute hypotension) and Figure 2 (sepsis). It can be observed that the synthetic data generated by CA-GAN exhibits significant overlap with the real

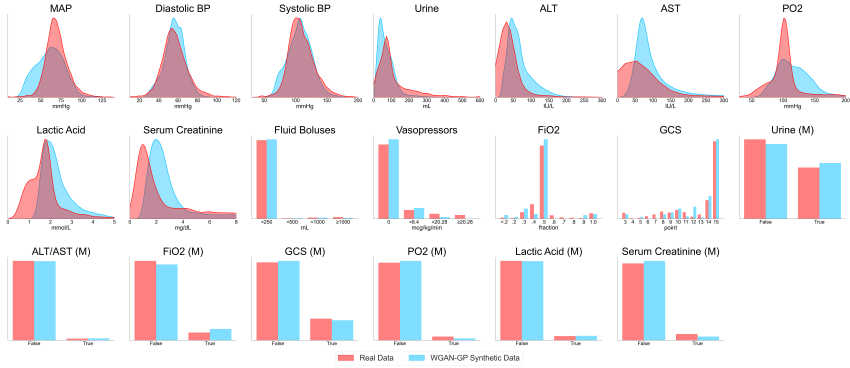
data, indicating our model’s ability to capture the underlying structure accurately. In contrast, WGAN-GP* and SMOTE exhibit different characteristics. SMOTE’s interpolation of real data points fills the gaps between the closest points without expanding into the embedded space, potentially compromising data authenticity. On the other hand, CA-GAN distributes data points uniformly throughout the space while adhering to the constraints of the real distribution. This suggests that our model improves generalisation in the data space. For sepsis dataset, SMOTE displays similar behaviour to acute hypotension, interpolating real data points. In contrast, our CA-GAN achieves better results by showcasing a substantial overlap between real and synthetic data without the interpolation effect. While WGAN-GP* shows some improvement, its distribution still exhibits visible areas where the distributions do not overlap.

Subsequently, PCA-based analysis shows that CA-GAN can generate data points covering the entire variance of the real data. At the same time, SMOTE and WGAN-GP* tend to converge on the mean, flattening their variance as shown in the middle panels of Figure 1 for acute hypotension and Figure 2 for sepsis. We also present the UMAP latent representation of the data, which like PCA, preserves the global structure in the bottom panels of Figures 1 and 2 with similar observations. State of the art WGAN-GP* appears to suffer from mode collapse, a significant limitation of GANs [32]. Mode collapse occurs when the generator produces a limited variety of samples despite being trained on a diverse dataset. The generator cannot fully capture the complexity of the target distribution, limiting the quantity of generated samples and resulting in repetitive output. This is because the generator can get stuck in a local minimum where a few outputs are repeatedly generated, even though the training data contains more modes that can be learned. This presents a significant challenge in generating high-quality, authentic samples, while our CA-GAN model overcomes this limitation.

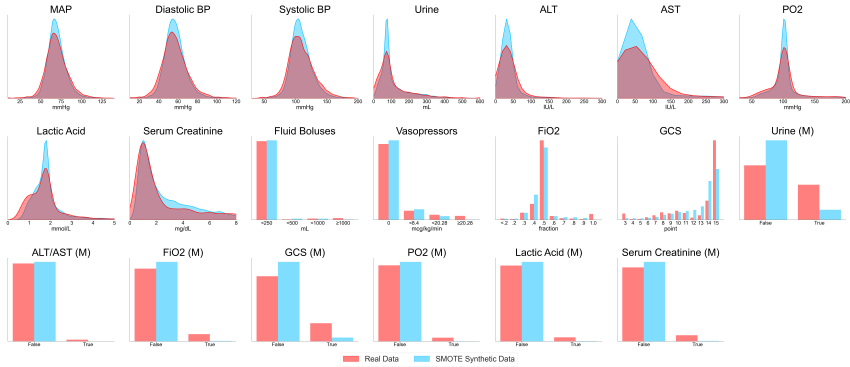
Finally, we show the distribution of individual variables of synthetic data overlaid on the distribution of the real data to compare the three methods for the acute hypotension dataset in Figure 3 and sepsis in Appendix A. Joint distributions are shown in Appendix D). The distribution of synthetic data generated by our CA-GAN exhibits the closest match to that of the real data. This close alignment is particularly evident in variables related to blood pressure, including MAP, diastolic, and systolic measurements. However, certain variables, such as urine and ALT/AST, pose challenges for all three methods. These variables have highly skewed distributions with long tails, making them difficult to transform effectively using power or logarithmic transformations. In contrast, our CA-GAN and WP-GAN* effectively capture the distribution of categorical variables. Conversely, SMOTE encounters difficulties with several variables, including both the numeric variable of urine and the categorical variable of the Glasgow Coma Score (GCS). These observations are also reflected in the quantitative evaluation in Section 2.2. The variables in the sepsis dataset are not only more than twice as many as those in acute hypotension but also have more complex distributions. Variables such as SGOT, SGPT, total bilirubin,



(a) CA-GAN



(b) WGAN-GP*



(c) SMOTE

Fig. 3: Distribution plots of each variable, overlaying real and synthetic data for acute hypotension dataset. Distribution of variables related to blood pressure (MAP, diastolic and systolic) is captured well by our method in comparison to WGAN-GP* and SMOTE. CA-GAN performs better also for categorical variables, while all the three methods struggle with variables with long tail distributions.

maximum dose of vasopressors, and others have extremely long tails. The three methods struggle to generate these kinds of distributions and show a tendency to converge to the median value. In contrast, the behaviour is similar to acute hypotension for categorical and numerical variables normally distributed.

2.2 Quantitative evaluation

We used Kullback-Leibler (KL) divergence [33] to measure the similarity between the discrete density function of the real data and that of the synthetic data. For each variable v of the dataset, we calculate:

$$D_{KL}(P_v \| Q_v) = \sum_i P_v(i) \log \frac{P_v(i)}{Q_v(i)} \quad (1)$$

where Q_v is the true distribution of the variable and P_v is the generated distribution. The smaller the divergence, the more similar the distributions; zero indicates identical distributions. The left half of Tables 1a and 1b show the results of the KL divergence for each variable. Our CA-GAN method has the lowest median across all variables for acute hypotension and sepsis data compared to WGAN-GP* and SMOTE. This is despite the fact that SMOTE is specifically designed to maintain the distribution of the original variables.

In addition, we used Maximum Mean Discrepancy (MMD) [34] to calculate the distance between the distributions based on kernel embeddings, that is, the distance of the distributions represented as elements of a reproducing kernel Hilbert space (RKHS). We used a Radial Basis Function (RBF) Kernel:

$$K(x_{real}, x_{syn}) = \exp \left(-\frac{\|x_{real} - x_{syn}\|^2}{2\sigma^2} \right) \quad (2)$$

with $\sigma = 1$. The right half of Tables 1a and 1b shows the MMD results for SMOTE, WGAN-GP* and our CA-GAN. Again, our model has the best median performance across all the variables for acute hypotension data, while for sepsis data, SMOTE shows a difference in performance by 0.00028. In summary, CA-GAN performs best in the acute hypotension dataset by a wide margin while showing comparable performance with SMOTE in the sepsis dataset.

2.3 Variable correlations

We used the Kendall rank correlation coefficient τ [35] to investigate whether synthetic data maintained original correlations between variables found in the real data of acute hypotension and sepsis datasets. This choice is motivated by the fact that the τ coefficient does not assume a normal distribution, which is the case for some of our variables, of the sepsis dataset in particular (as shown in Figure 3 and Appendix A). Figure 4 shows the results of Kendall's rank correlation coefficients. For the acute hypotension dataset (Figure 4a), CA-GAN captures the original variable correlations, as does SMOTE, with

Table 1: KL-Divergence and Maximum Mean Discrepancy between the distribution of real and synthetic data for each variable of the datasets.

	KL-divergence			MMD		
	SMOTE	WGAN-GP*	CA-GAN	SMOTE	WGAN-GP*	CA-GAN
MAP	0.11182	0.24941	0.17164	0.00137	0.00824	0.00110
Diastolic BP	0.28191	0.91622	0.24342	0.00155	0.00209	0.00086
Systolic BP	0.06405	0.10588	0.13194	0.00138	0.00120	0.00092
Fluid Boluses	0.01121	0.00358	0.00052	0.00047	0.00022	0.00003
Urine	0.00892	0.15183	0.00901	0.01321	0.08567	0.08443
Vasopressors	0.03622	0.05955	0.00175	0.00463	0.00883	0.00031
ALT	0.00068	0.37020	0.00800	0.01356	0.20156	0.18616
AST	0.00083	0.18162	0.00455	0.01323	0.20920	0.19538
FiO2	0.00858	0.01950	1.36841	0.00091	0.00043	0.00012
GCS	0.02432	0.02571	0.01934	0.05206	0.00688	0.00791
PO2	0.00315	0.13503	0.31726	0.00992	0.25091	0.24806
Lactic Acid	0.03192	0.42781	0.45402	0.01084	0.16273	0.19777
Serum Creatinine	0.02079	0.02851	0.08827	0.01892	0.22812	0.03313
Urine (M)	0.19717	0.00279	0.00070	0.09954	0.00170	0.00043
ALT/AST (M)	0.01872	0.00027	0.00031	0.00050	0.00001	0.00002
FiO2 (M)	0.07361	0.00965	0.00459	0.00892	0.00224	0.00103
GCS (M)	0.12043	0.00072	0.00013	0.03776	0.00030	0.00006
PO2 (M)	0.03846	0.00751	0.00033	0.00238	0.00067	0.00003
Lactic Acid (M)	0.03962	0.00010	0.00136	0.00274	0.00001	0.00015
Serum Creatinine (M)	0.05844	0.00777	0.00005	0.00613	0.00117	0.00001
Median	0.03407	0.02711	0.00629	0.00752	0.00217	0.00089

(a) Acute hypotension data

	KL-divergence			MMD		
	SMOTE	WGAN-GP*	CA-GAN	SMOTE	WGAN-GP*	CA-GAN
Age	0.01796	0.03107	0.02815	0.00543	0.00960	0.00849
Heart Rate	0.01140	0.07822	0.03885	0.00158	0.00438	0.00243
Systolic BP	0.12038	0.09645	0.08592	0.00144	0.00319	0.00262
Mean BP	0.08035	0.29433	0.27170	0.00192	0.01012	0.00286
Diastolic BP	0.16654	0.30986	0.39555	0.00186	0.00319	0.00186
Respiratory Rate	0.03584	0.04324	0.04050	0.00395	0.00273	0.02020
Potassium	0.15016	0.11200	0.27340	0.00546	0.01811	0.00742
Sodium	0.22161	0.18242	0.19199	0.00372	0.01702	0.00124
Chloride	0.03949	0.06267	0.00989	0.00291	0.00410	0.00403
Calcium	0.33564	0.16861	0.13301	0.00604	0.06938	0.00585
Ionised Ca	1.88754	0.07055	0.01103	0.00005	0.90096	0.77536
CO2	0.04157	0.09045	0.05244	0.00371	0.00170	0.00118
Albumin	0.01604	0.00967	0.00532	0.00719	0.01420	0.00534
Hemoglobin	0.44026	0.30347	0.20345	0.00612	0.04899	0.02199
pH	0.12049	0.30020	0.08537	0.00002	0.00215	0.00003
Arterial Base Excess	0.14158	0.12252	0.04117	0.00410	0.01532	0.01113
HCO3	0.02426	0.12058	0.01444	0.00387	0.01526	0.00256
FiO2	0.01122	0.03122	0.03055	0.00022	0.00480	0.00160
Glucose	0.02167	0.12281	0.11088	0.00075	0.00041	0.00085
Blood Urea Nitrogen	0.04561	0.06180	0.05283	0.00211	0.00440	0.00391
Creatinine	0.00403	0.02395	0.13305	0.00739	0.04867	0.01437
Magnesium	0.05638	0.33564	0.18024	0.00158	0.04239	0.00214
SGOT	0.00104	0.00859	0.00199	0.00229	0.00907	0.00223
SGPT	0.00152	0.01028	0.00277	0.00198	0.00459	0.00340
Total Bilirubin	0.00493	0.02875	0.02077	0.00900	0.11124	0.00337
WBC	0.13135	0.08064	0.00788	0.00328	0.00573	0.02103
Platelets Count	0.00717	0.07344	0.00397	0.00116	0.00120	0.00079
paO2	0.01067	0.27433	0.02362	0.00091	0.00321	0.00071
paCO2	0.01632	0.05257	0.15250	0.00145	0.00729	0.00113
Lactate	0.00228	0.19152	0.11907	0.00829	0.01251	0.00342
Input Fluids Total	0.01047	0.00990	0.01833	0.00116	0.00208	0.00190
Input 4H	0.00397	0.00481	0.00471	0.02146	0.04044	0.02819
Max Vasopressors 4H	0.00886	0.00240	0.00295	0.00028	0.00083	0.00133
Total Urine Output	0.01397	0.01009	0.00832	0.00395	0.01644	0.01511
Output 4H	0.03328	0.00800	0.00484	0.00947	0.04256	0.02401
Gender	0.00117	0.02196	0.01476	0.01363	0.01384	0.00931
Readmission of Patient	0.00091	0.02287	0.01917	0.00064	0.01346	0.01134
Mechanical Ventilation	0.00065	0.02689	0.00577	0.00054	0.01685	0.00364
Temperature	0.00035	0.01592	0.00722	0.00011	0.00336	0.00236
GCS	0.01751	0.06029	0.01191	0.02948	0.02881	0.00903
SpO2	0.03123	0.09465	0.06963	0.02013	0.04669	0.03336
PTT	0.02686	0.03667	0.02221	0.01405	0.01906	0.01723
PT	0.03676	0.03933	0.00986	0.02061	0.03367	0.00594
INR	0.02486	0.03850	0.00669	0.02113	0.01912	0.00568
Median	0.02296	0.06105	0.02292	0.00349	0.01299	0.00377

(b) Sepsis data

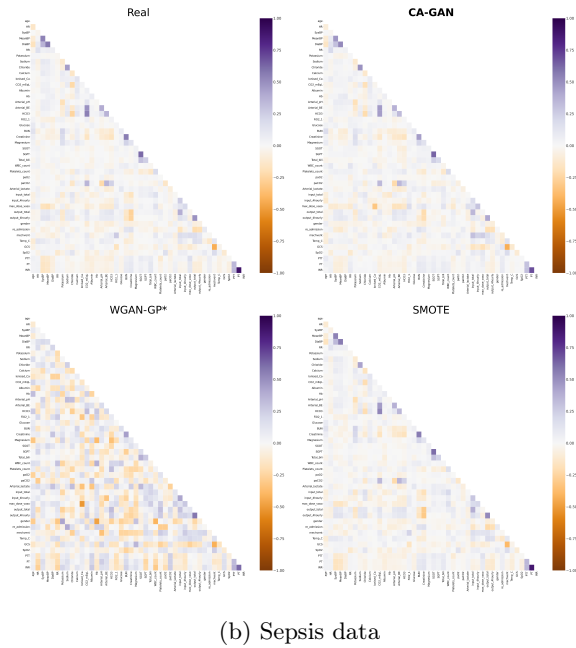
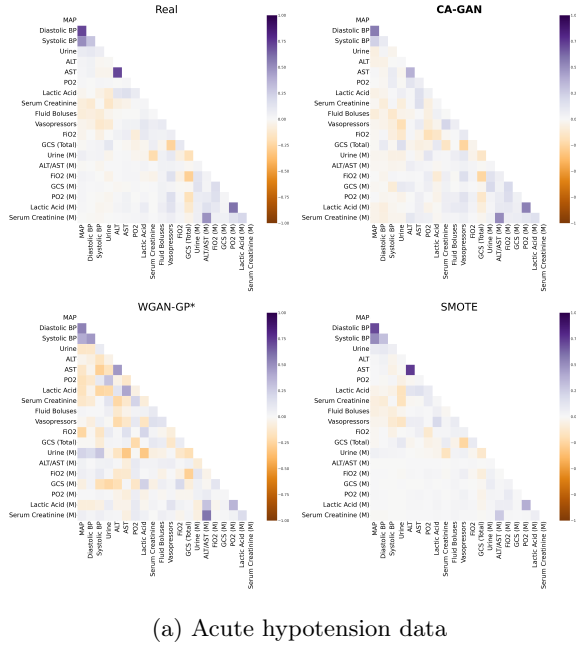


Fig. 4: Kendall's rank correlation coefficients for the real data and the data generated with CA-GAN, WGAN-GP*, and SMOTE.

the former having the closest results on categorical variables, while the latter on numerical ones. WGAN-GP* shows the worst performance, accentuating correlations that do not exist in real data. Similar patterns are also obtained for the variables of patients with sepsis in Figure 4b.

2.4 Synthetic data authenticity

When generating synthetic data, the output must be a realistic representation of the original data. Still, we also need to verify that the model has not merely learned to copy the real data. GANs are prone to overfitting by memorising the real data [36]; therefore, we use Euclidean Distance (L_2 Norm) to evaluate the originality of our model's output. Our analysis shows that the smallest distance between a synthetic and a real sample is 52.6 for acute hypotension and 44.2 for sepsis, indicating that the generated synthetic data are not a mere copy of the real data. This result, coupled with the visual representation of CA-GAN (shown in Figure 1 and 2), illustrates the ability of our model to generate authentic data. SMOTE, which by design interpolates the original data points, is unable to explore the underlying multidimensional space. Therefore its generated data samples are much closer to the real ones, with a minimum Euclidean distance of 0.0023 for acute hypotension and 0.033 for sepsis. A summary of distance metrics, including median, mean, standard deviation, maximum and minimum is shown in Appendix E, Tables E3a and E3b.

2.5 Downstream regression task

Finally, we also sought to evaluate the ability of CA-GAN to maintain the temporal properties of time series data, considering ethnicity (shown here) and gender (shown in Appendix G). Since our objective is to augment the minority class to mitigate representation bias, we wanted to verify that the datasets augmented with synthetic data generated by our model can maintain or improve the predictive performance of the original data on a downstream task. Initially, we trained only a Bidirectional Long Short-Term Memory (BiLSTM) with real data as the baseline. Later, we trained the BiLSTM with synthetic and augmented datasets separately, considering ethnicity and gender diversity. They were used to evaluate the performance in a regression task. A complete description of how we performed these experiments is provided in Appendix F.

Table 2a and Table 2b show the mean absolute errors between the BiLSTM prediction and the actual acute hypotension and sepsis observations, respectively; additionally, Table G4 shows the results we obtained with data conditioned on gender. In the first column, we show the results achieved using only the real data to make the predictions; in the second column, the results using only the synthetic data; and finally, in the third column, the results achieved by predicting with the augmented dataset, that is, with both the real and synthetic data together, considering both ethnic and gender diversity in the augmentation process. Overall, adding the synthetic data reduces the predictive error. This indicates that the temporal characteristics of the data

12 *Mitigating Representation bias***Table 2:** Mean prediction errors of a BiLSTM trained on real, synthetic, and augmented data for a downstream prediction task. The numbers in parentheses represent the standard deviation

	Real	Synthetic	Augmented
MAP	10.129 (0.487)	9.084 (0.401)	8.530 (0.234)
Diastolic BP	8.328 (0.653)	7.500 (0.246)	7.491 (0.205)
Systolic BP	19.930 (0.752)	16.375 (1.405)	13.121 (0.646)
Fluid Boluses	19.547 (2.387)	22.987 (2.051)	22.684 (1.544)
Urine	54.915 (1.591)	49.615 (2.201)	49.461 (3.279)
Vasopressors	0.290 (0.051)	0.446 (0.079)	0.430 (0.082)
ALT	7.561 (0.616)	8.244 (1.079)	6.235 (2.018)
AST	18.017 (3.876)	9.629 (2.106)	8.091 (2.377)
FIO ₂	0.022 (0.019)	0.023 (0.008)	0.028 (0.015)
GCS	0.226 (0.069)	0.481 (0.093)	0.666 (0.177)
PO ₂	26.745 (9.310)	12.297 (1.184)	11.375 (4.392)
Lactic Acid	0.107 (0.064)	0.262 (0.018)	0.168 (0.023)
Serum Creatinine	0.158 (0.054)	0.357 (0.037)	0.321 (0.040)
Median	8.493 (0.639)	8.255 (0.731)	6.844 (0.843)

(a) Acute hypotension data

	Real	Synthetic	Augmented
Heart Rate	13.926 (1.406)	6.462 (0.510)	6.061 (0.238)
Systolic BP	20.975 (0.411)	12.129 (1.048)	11.636 (0.704)
Mean BP	12.628 (0.885)	7.706 (0.376)	7.447 (0.458)
Diastolic BP	9.793 (0.468)	8.427 (0.286)	8.282 (0.446)
Respiratory Rate	2.515 (0.270)	2.388 (0.065)	2.341 (0.039)
Potassium	0.183 (0.020)	0.207 (0.027)	0.220 (0.048)
Sodium	28.981 (1.978)	3.698 (0.077)	3.733 (0.122)
Chloride	8.125 (0.396)	4.533 (0.368)	4.080 (0.483)
Calcium	0.388 (0.043)	0.327 (0.057)	0.388 (0.118)
Ionised Ca	0.052 (0.001)	0.092 (0.043)	0.086 (0.041)
Carbon Dioxide	2.324 (0.206)	2.033 (0.177)	1.893 (0.158)
Albumin	0.516 (0.006)	0.452 (0.020)	0.442 (0.008)
Hemoglobin	0.725 (0.087)	0.616 (0.063)	0.655 (0.079)
pH	0.082 (0.050)	0.083 (0.022)	0.075 (0.041)
Arterial Base Excess	2.972 (0.070)	2.876 (0.019)	2.847 (0.019)
HCO ₃	3.244 (0.628)	2.391 (0.065)	2.457 (0.142)
FIO ₂	0.068 (0.025)	0.063 (0.016)	0.046 (0.014)
Glucose	34.395 (0.765)	24.366 (0.543)	23.388 (0.765)
Blood Urea Nitrogen	4.096 (0.765)	4.484 (0.429)	3.430 (0.343)
Creatinine	0.135 (0.035)	0.257 (0.056)	0.276 (0.041)
Magnesium	0.109 (0.015)	0.126 (0.023)	0.126 (0.031)
SGOT	216.348 (2.019)	206.530 (0.731)	207.164 (1.537)
SGPT	165.979 (1.735)	153.379 (1.475)	153.672 (1.527)
Total Bilirubin	1.550 (0.089)	1.457 (0.155)	1.398 (0.028)
WBC	1.072 (0.208)	1.516 (0.144)	1.264 (0.097)
Platelets Count	119.777 (4.692)	59.953 (4.340)	62.003 (6.094)
paO ₂	37.749 (0.064)	35.157 (1.201)	35.318 (1.989)
paCO ₂	7.206 (0.454)	6.156 (0.377)	6.035 (0.292)
Lactate	1.026 (0.174)	0.864 (0.024)	0.860 (0.018)
Input Fluids Total	9824.288 (6.460)	9378.006 (56.594)	9354.273 (27.237)
Input 4H	195.774 (1.827)	177.704 (1.970)	178.058 (4.157)
Max Vasopressors 4H	0.048 (0.018)	0.085 (0.043)	0.126 (0.144)
Total Urine Output	9067.905 (4.940)	8738.295 (16.576)	8770.296 (29.386)
Output 4H	235.173 (4.450)	169.318 (5.368)	168.216 (4.849)
Median	3.932 (0.536)	2.876 (0.019)	2.847 (0.019)

(b) Sepsis data

generated by our CA-GAN model are close enough to those of the real data to maintain the original predictive performance. Thus, the augmented dataset could be used in a downstream task, mitigating the representation bias. Similar findings are also shown for the gender-augmented dataset in Appendix G.

It should be noted that the errors in Input Fluids Total and Total Urine Output are exceptionally high compared to the other variables. This is because

predicting these variables is generally challenging, stemming partly from how they are collected and recorded rather than an issue inherent to synthetic data generation.

3 Discussion

As machine intelligence scales upwards in clinical decision-making, the risk of perpetuating existing health inequities increases significantly. This is because biased decision-making can continuously feed back the data used to train the models, creating a vicious circle that further ingrains discrimination towards underrepresented groups. Representation bias, in particular, frequently occurs in health data, leading to decisions that may not be in the best interests of all patients, favouring specific sub-populations while treating underrepresented sub-populations, such as those with standard set characteristics including ethnicity, gender, and disability unfavourably.

To address these issues, representation must be improved before algorithmic decision-making becomes integral to clinical practice. While unequal representation is a multifaceted challenge involving diverse factors such as socio-economic, cultural, systemic, and data, our work represents a step towards addressing one significant facet of this challenge: existing representation bias in health data.

We have shown that our work can improve representation bias when evaluated against state-of-the-art architectures and traditional approaches such as SMOTE. SMOTE has notable advantages over other data generation techniques as it requires no training and can generate data instantly, making it an efficient approach. SMOTE demonstrates better performance than other methods when dealing with complex numerical distributions. It can create non-normal distributions even if it tends to overestimate the median in long-tail distributions. This is in contrast to GANs, which struggle with these types of distributions. Moreover, SMOTE maintains a correlation between the variables as the generated data is similar to the original due to interpolation. In turn, generating authentic data remains a significant challenge for SMOTE.

Through qualitative and quantitative evaluation, we have shown that CA-GAN can generate authentic data samples with high distribution coverage, avoiding mode collapse failure, while ensuring that the generated data are not copies of the real data. We have also shown that augmenting the dataset with the synthetic data generated by CA-GAN leads to lower errors in the downstream regression task. This indicates that our model can generalise well from the original data.

A notable advantage of our approach is that it uses the overall dataset, and not only the minority class, as is the case with WGAN-GP* and SMOTE. This means that CA-GAN can be applied in smaller datasets and those with highly imbalanced classes, such as rare diseases.

Furthermore, we evaluated our method on two datasets with diverse characteristics and found that our CA-GAN performed better on the acute hypotension dataset. This may be because some of the numerical variables in the sepsis

dataset have long-tailed distributions, presenting a modelling challenge for all the methods. Additionally, the sepsis dataset contained fewer data points per patient than acute hypotension (15 versus 48 observations). A shorter input sequence may have created difficulty for BiLSTM modules to learn the underlying structure of the original data effectively, coupled with a higher number of variables (twice as many) in the sepsis dataset. We also note that the lower number of patients in the acute hypotension dataset does not impact the generative performance of our method. This ability to work with fewer data points (patients) is encouraging, given the overall objective of our goal of augmenting representation.

In a comprehensive comparison to state-of-the-art methods and computationally inexpensive approaches, CA-GAN architecture showed superior performance while also considering some of the limitations of our work. CA-GAN may require additional optimisation to further increase performance on datasets with variables with long-tailed distribution and lower data points per patient. Furthermore, additional analysis will be necessary to evaluate the generalisation capability of our architecture beyond clinical data.

Looking forward, we aim to refine CA-GAN, exploring alternative architectures, and ensuring adaptability to diverse datasets, allowing its effective use in real-world applications.

The implementation of multiple BiLSTM layers within the CA-GAN framework, while beneficial for capturing the nuances of sequential data, does introduce a degree of model complexity that can be computationally demanding. An exploration into alternative methods such as convolutional neural networks (CNNs) or Temporal Convolutional Networks (TCNs) presents a promising direction to potentially improve the efficiency of our model. The work of Bai et al. [37] provides an empirical foundation for this approach, indicating that such network structures can rival the performance of recurrent networks for sequence modelling tasks. Additionally, prior research [38] suggests that simplifying the internal mechanisms of these recurrent units can lead to improvements in both performance and computational efficiency. These insights provide a strong impetus for our future work, where we aim to refine the CA-GAN model to harness the benefits of these alternative architectures without compromising its ability to perform conditional generation.

The phenomenon of mode collapse, particularly prevalent in scenarios involving imbalanced categorical data, remains a significant challenge for GAN architectures. In response, we are considering an approach inspired by the methodologies of ADASYN [39] and SMOTE, which use clustering techniques to enhance data diversity. By generating additional synthetic data within clusters of similar features and adjusting the dataset composition based on cluster size, we aim to create more representative and balanced synthetic datasets. This strategy holds the potential to mitigate the risks associated with mode collapse and improve the robustness of the CA-GAN's output.

The task of generalising to unseen data categories is particularly challenging due to the inherent unknowns these categories represent. While a definitive

strategy is yet to be developed, we believe that integrating conditional generation with metric learning, as seen in prototypical networks [40], could provide a dual advantage. This integration could not only facilitate the generation of novel data points but also offer a quantifiable framework to assess their similarity or dissimilarity to known data categories. Such an approach could extend the capabilities of CA-GAN beyond data augmentation, potentially improving the interpretability and applicability of the synthetic data generated.

In terms of evaluation metrics, our current approach primarily focuses on statistical properties of the generated data. However, to ascertain the practical utility and accuracy of the synthetic data produced by CA-GAN, we recognize the importance of domain-specific validations, including performance in sub-populations [41, 42]. Inspired by the collaborative efforts outlined in [43], we are committed to forging partnerships with experts in relevant fields such as healthcare and clinical practice. These domain experts, with their invaluable insights and practical knowledge, will be crucial in guiding the development of evaluation metrics. Their input will ensure that our synthetic datasets can meet the rigorous demands of real-world applications and contribute meaningfully to the domains they are intended to serve.

Lastly, our architecture can provide a solid basis to generate privacy preserving synthetic data and mitigate barriers associated with access to clinical data. This is because, we have ensured that the synthetic data generated by our CA-GAN are not a mere copy of the real data on one hand, while on the other, the synthetic data reflect the distributions of the real data. However, privacy preserving analysis will require additional analysis, such as reconstruction attacks, which are beyond the scope of the current work.

4 Methods

We begin by formally formulating the problem we are addressing. Then we discuss the data sources we used to train our models and compare and contrast Generative Adversarial Networks (GANs) and Conditional Generative Adversarial Networks (CGANs). We also provide an in-depth analysis of the baseline model for this work, WGAN-GP*. Finally, we present the architecture of our proposed Conditional Augmentation GAN (CA-GAN) and discuss its advantages over other methods.

4.1 Problem Formulation

Let A be a vector space of features and let $a \in A$ represent a feature vector. Let $L = \{0, 1\}$ be a binary distribution modifier, and let l a binary mask extracted from L . We consider a data set $D_0 = \{a_n\}_{n=1}^N$ with $l = 0$, where individual samples are indexed by $n \in \{1, \dots, N\}$ and we also consider a data set $D_1 = \{a_m\}_{m=N+1}^{N+M}$ with $l = 1$, where individual samples are indexed by $m \in \{N+1, \dots, N+M\}$, and $N > M$. We define the training data set D as $D = D_0 \cup D_1$.

Our goal is to learn a density function $\hat{d}\{A\}$ that approximates the true distribution $d\{A\}$ of D . We also define $\hat{d}_l\{A\}$ as $\hat{d}\{A\}$ with $l = 1$ applied.

To balance the number of samples in D , we draw random variables X from $\hat{d}_1\{A\}$ and add them to D_1 until $N = M$. Thus, we balance out D .

4.2 Data sources, variables and patient population

In this work, we want to generate tabular datasets with a complex structure: longitudinal, multivariate, and different data types. We chose two datasets extracted from the MIMIC-III database. The inclusion and exclusion criteria are described in the literature [44, 45]. In addition, these two datasets have already been used in previous studies [27]. We decided to test the methods for the oversampling of only one minority class, thus discarding for the time being patients who did not belong to the Caucasian or Black ethnic groups. We used a similar approach for gender, shown in Appendix G.

The acute hypotension dataset comprises 3343 patients admitted to critical care; the patients were either of Black (395) or Caucasian (2948) ethnicity. Each patient is represented by 48 data points, corresponding to the first 48 hours after the admission, in addition to 9 numeric, four categorical, and seven binary variables (20 in total). Details of the dataset are presented in Appendix B, Table B1.

The Sepsis dataset comprises 4192 patients admitted to critical care of either Black (461) or Caucasian (3731) ethnicity. Each patient is represented by 15 data points, corresponding to observations taken every 4 hours from admission, in addition to 35 numeric, six categorical, and three binary variables (44 in total). Details of the dataset are presented in Appendix B, Table B2.

4.3 GAN vs CGAN

The Generative Adversarial Network (GAN) [46] entails two components: a generator and a discriminator. The generator G is fed a noise vector z taken from a latent distribution p_z and outputs a sample of synthetic data. The discriminator D inputs either fake samples created by the generator or real samples x taken from the true data distribution p_{data} . Hence, the GAN can be represented by the following minimax loss function:

$$\min_G \max_D V(D, G) = \mathbb{E}_{x \sim p_{data}(x)} [\log D(x)] + \mathbb{E}_{z \sim p_z(z)} [1 - \log D(G(z))] \quad (3)$$

The goal of the discriminator is to maximise the probability of discerning fake from real data, whilst the purpose of the generator is to make samples realistic enough to fool the discriminator, i.e., to minimise $\mathbb{E}_{z \sim p_z(z)} [1 - \log D(G(z))]$. As a result of the reciprocal competition, both the generator and discriminator improve during training.

The limitations of vanilla GAN models become evident when working with highly imbalanced datasets, where there might not be sufficient samples to train the models to generate minority-class samples. A modified version of GAN, the

Conditional GAN [47], solves this problem using labels y in both the generator and discriminator. The additional information y divides the generation and the discrimination in different classes. Hence, the model can now be trained on the whole dataset to generate only minority-class samples. Thus, the loss function is modified as follows:

$$\min_G \max_D V(D, G) = \mathbb{E}_{x \sim p_{\text{data}}(x)} [\log D(x||y)] + \mathbb{E}_{z \sim p_z(z)} [1 - \log D(G(z||y))] \quad (4)$$

GAN and CGAN, overall, share the same significant weaknesses during training, namely mode collapse and vanishing gradient [32]. In addition, as GANs were initially designed to generate images, they have been shown unsuitable for generating time-series [48] and discrete data samples [49].

4.4 WGAN-GP*

The WGAN-GP* introduced by Kuo et al. [27] solved many of the limitations of vanilla GANs. The model was a modified version of a WGAN-GP [25, 26]; thus, it applied the Earth Mover distance (EM) [50] to the distributions, which had been shown to solve both vanishing gradient and mode collapse [51]. In addition, the model applied the Gradient Penalty during training, which helped to enforce the Lipschitz constraint on the discriminator efficiently. In contrast with vanilla WGAN-GP, WGAN-GP* employed soft embeddings [52, 53], which allowed the model to use inputs as numeric vectors for both binary and categorical variables, and a Bidirectional LSTM layer [54, 55], which allowed for the generation of samples in time-series. While L_D was kept the same, L_G was modified by Kuo et al. [27] by introducing alignment loss, which helped the model to capture correlation among variables over time better. Hence, the loss functions of WGAN-GP* are the following:

$$L_D = \mathbb{E}_{z \sim p_z(z)} [D(G(z))] - \mathbb{E}_{x \sim p_{\text{data}}(x)} [D(x)] + \lambda_{GP} \mathbb{E}_{z \sim p_z(z)} [(\nabla D(G(z)))_2 - 1]^2 \quad (5)$$

$$L_G = -\mathbb{E}_{z \sim p_z(z)} [D(G(z))] + \underbrace{\lambda_{corr} \sum_{i=1}^n \sum_{j=1}^{i-1} \|r_{syn}^{(i,j)} - r_{real}^{(i,j)}\|_{L_1}}_{\text{Alignment loss}} \quad (6)$$

To calculate alignment loss, we computed Pearson's r correlation [56] for every unique pair of variables $X^{(i)}$ and $X^{(j)}$. We then applied the L_1 loss to the differences in the correlations between r_{syn} and r_{real} , with λ_{corr} representing a constant acting as a strength regulator of the loss.

In their follow-up papers, Kuo et al. noted that their simulated data based on their proposed WGAN-GP* lacked diversity. In [57], the authors found that WGAN-GP* continued to suffer from mode collapse like the vanilla GAN. Similar to our own CA-GAN, the authors extended the WGAN-GP setup with a conditional element where they externally stored features of the real data during training and replayed them to the generator sub-network at test time.

In [58], the same panel of researchers also experimented with diffusion models [59] and found that diffusion models better represent binary and categorical variables. Nonetheless, they demonstrated that GAN-based models encoded less bias (in the means and variances) of the numeric variable distributions.

4.5 CA-GAN

We built our CA-GAN by conditioning the generator and the discriminator on static labels y . Hence, the updated loss functions used by our model are as follows:

$$L_D = \mathbb{E}_{z \sim p_z(z)}[D(G(z||y))] - \mathbb{E}_{x \sim p_{\text{data}}(x)}[D(x||y)] + \lambda_{GP} \mathbb{E}_{z \sim p_z(z)}[(\nabla D(G(z||y)))_2 - 1]^2 \quad (7)$$

$$L_G = -\mathbb{E}_{z \sim p_z(z)}[D(G(z||y))] + \underbrace{\lambda_{corr} \sum_{i=1}^n \sum_{j=1}^{i-1} \|r_{syn}^{(i,j)} - r_{real}^{(i,j)}\|_{L_1}}_{\text{Alignment loss}} \quad (8)$$

Where y can be any categorical label. During training, the label y was used to differentiate the minority from the majority class, and during generation, they were used to create fake samples of the minority class.

Compared to WGAN-GP* we also increased the number of BiLSTMs from 1 to 3 both in the generator and the discriminator, as stacked BiLSTMs have been shown to capture complex time-series better [60]. In addition, we decreased the learning rate and batch size during training. An overview of the CA-GAN architecture is shown in Figure 5.

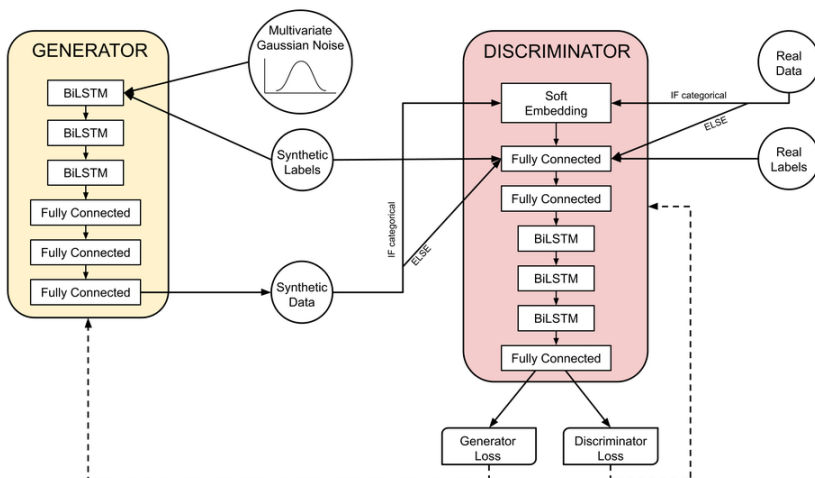


Fig. 5: Proposed architecture of our CA-GAN.

Declarations

4.6 Funding

None

4.7 Competing interests

None

4.8 Ethics approval

The data in MIMIC-III was previously de-identified, and the institutional review boards of the Massachusetts Institute of Technology (No. 0403000206) and Beth Israel Deaconess Medical Center (2001-P-001699/14) both approved the use of the database for research.

4.9 Availability of data and materials

The data underlying this article are publicly available in the MIMIC-III repository (<https://mimic.physionet.org/>).

4.10 Code availability

The source code will be made available upon publication at the github repository: <https://github.com/nic-olo/CA-GAN>

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Appendix A Distribution Plots for Sepsis

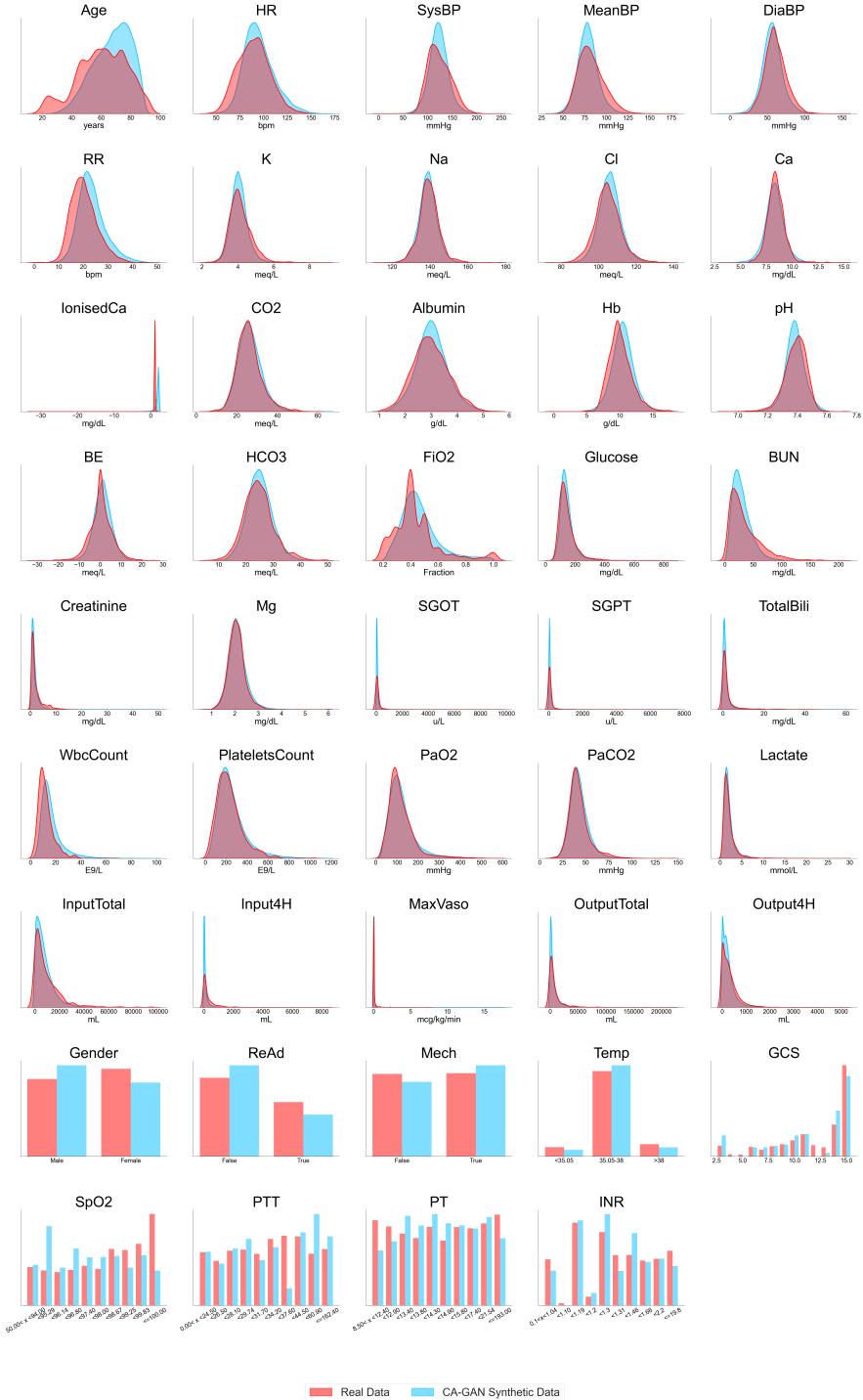


Fig. A1: Overlaid distribution plots of real data and CA-GAN synthetic data for each variable in the sepsis dataset.



Fig. A2: Overlaid distribution plots of real data and WGAN-GP* synthetic data for each variable in the sepsis dataset.

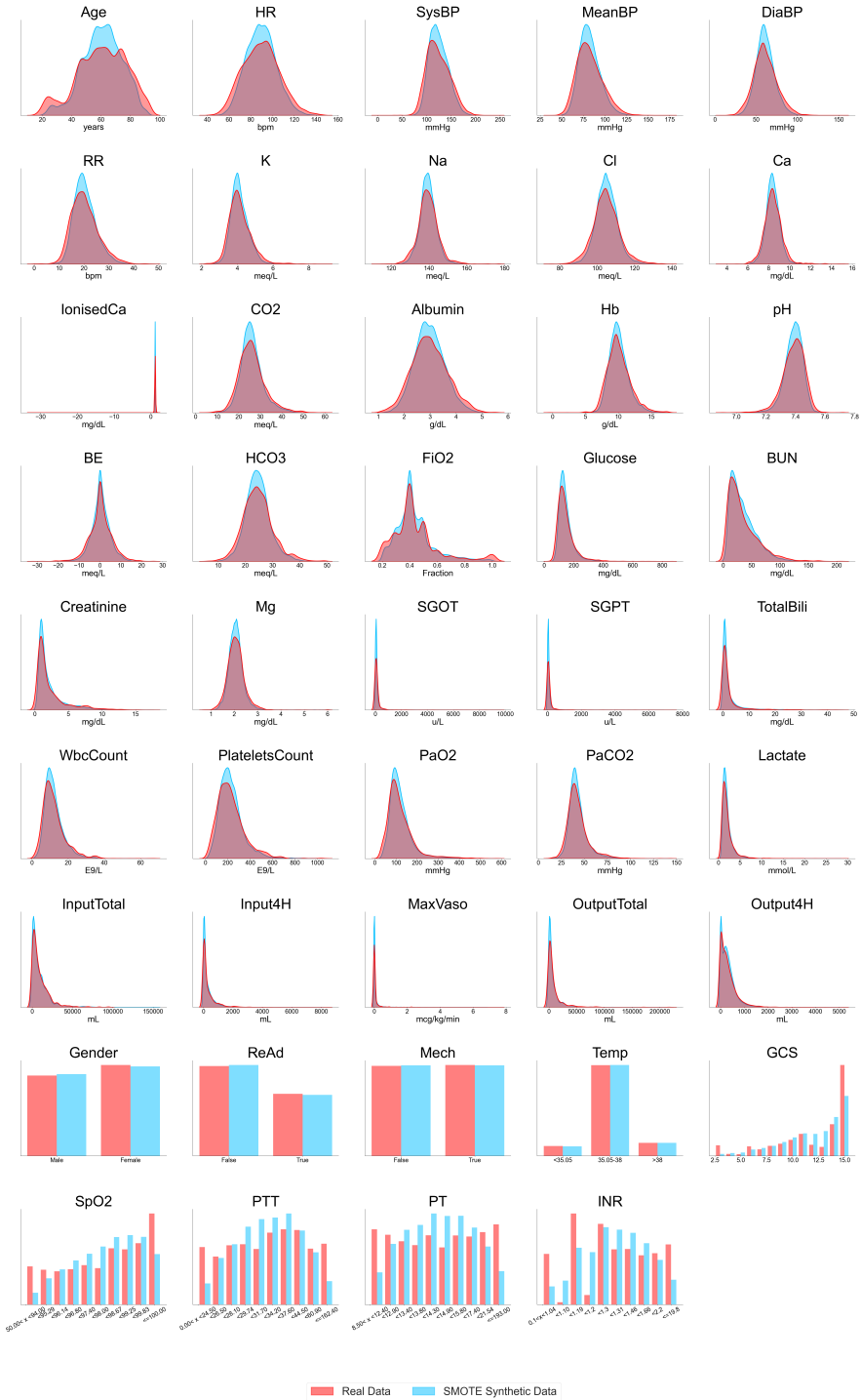


Fig. A3: Overlaid distribution plots of real data and SMOTE synthetic data for each variable in the sepsis dataset.

Appendix B Datasets

Table B1: Variables in the acute hypotension dataset. For each variable, the data type, the unit in which it is expressed, and the distribution statistics are presented.

Variable Name	Data Type	Unit	Descriptive Statistics	
Mean Arterial Pressure	numeric	mmHg	Median: 68.00 (Q1: 61.00, Q3: 76.00)	
Diastolic Blood Pressure	numeric	mmHg	Median: 54.00 (Q1: 47.00, Q3: 62.00)	
Systolic BP	numeric	mmHg	Median: 107.00 (Q1: 96.00, Q3: 120.00)	
Urine	numeric	mL	Median: 75.00 (Q1: 45.00, Q3: 140.00)	
Alanine Aminotransferase	numeric	IU/L	Median: 35.00 (Q1: 23.00, Q3: 35.00)	
Aspartate Aminotransferase	numeric	IU/L	Median: 50.00 (Q1: 33.00, Q3: 50.00)	
Partial Pressure of Oxygen	numeric	mmHg	Median: 102.00 (Q1: 99.00, Q3: 102.00)	
Lactate	numeric	mmol/L	Median: 1.80 (Q1: 1.20, Q3: 1.80)	
Serum Creatinine	numeric	mg/dL	Median: 1.10 (Q1: 0.80, Q3: 1.90)	
Fluid Boluses	categorical	mL	4 Classes [0,250) : 95.75%; [250,500) : 0.61% [500,1000) : 1.73%; ≥ 1000 : 1.91%	
Vasopressors	categorical	mcg/kg/min	4 Classes 0 : 81.95%; (0,8.4) : 9.02% [8.4,20.28) : 4.51%; ≥ 20.28 : 4.52%	
Fraction of Inspired Oxygen	categorical	fraction	10 Classes ≤ 0.2 : 0.44%; 0.2 : 0.45% 0.3 : 5.29%; 0.4 : 15.52% 0.5 : 61.64%; 0.6 : 4.36% 0.7 : 2.78%; 0.8 : 1.43% 0.9 : 1.42%; 1.0 : 6.67%	
Glasgow Coma Scale Score	categorical	point	13 Classes 3 : 4.57% 4 : 0.72% 5 : 0.44% 6 : 2.37% 7 : 3.44% 8 : 4.03% 9 : 3.63% 10 : 6.61% 11 : 4.48% 12 : 1.22% 13 : 3.23% 14 : 11.48% 15 : 53.80%	
Urine Data Measured (M)	binary	-	False: 55.64%	True: 44.36%
ALT or AST (M)	binary	-	False: 97.73%	True: 2.27%
FiO2 (M)	binary	-	False: 88.80%	True: 11.20%
GCS (M)	binary	-	False: 78.06%	True: 21.94%
PaO2 (M)	binary	-	False: 95.45%	True: 4.55%
Lactic Acid (M)	binary	-	False: 95.61%	True: 4.39%
Serum Creatinine (M)	binary	-	False: 92.79%	True: 7.21%

Table B2: Variables in the sepsis dataset. For each variable, the data type, the unit in which it is expressed, and the distribution statistics are presented.

Variable Name	Data Type	Unit	Descriptive Statistics
Age	numerical	years	Median: 66.95 (Q1: 54.21, Q3: 78.70)
Heart Rate (HR)	numerical	bpm	Median: 86.75 (Q1: 75.40, Q3: 98.86)
Systolic BP	numerical	mmHg	Median: 118.17 (Q1: 105.33, Q3: 134.20)
Mean BP	numerical	mmHg	Median: 77.25 (Q1: 69.12, Q3: 87.00)
Diastolic BP	numerical	mmHg	Median: 56.81 (Q1: 48.60, Q3: 65.67)
Respiratory Rate (RR)	numerical	bpm	Median: 20.00 (Q1: 16.86, Q3: 23.83)
Potassium (K)	numerical	meq/L	Median: 4.00 (Q1: 3.70, Q3: 4.30)
Sodium (Na)	numerical	meq/L	Median: 139.00 (Q1: 136.00, Q3: 142.00)
Chloride (Cl)	numerical	meq/L	Median: 105.00 (Q1: 101.00, Q3: 109.00)
Calcium (Ca)	numerical	mg/dL	Median: 8.30 (Q1: 7.84, Q3: 8.74)
Ionised Ca	numerical	mg/dL	Median: 1.13 (Q1: 1.08, Q3: 1.18)
Carbon Dioxide (CO2)	numerical	meq/L	Median: 26.00 (Q1: 22.75, Q3: 29.00)
Albumin	numerical	g/dL	Median: 2.90 (Q1: 2.50, Q3: 3.40)
Hemoglobin (Hb)	numerical	g/dL	Median: 10.00 (Q1: 9.04, Q3: 11.20)
pH	numerical	-	Median: 7.40 (Q1: 7.35, Q3: 7.44)
Arterial Base Excess	numerical	meq/L	Median: 0.00 (Q1: -2.00, Q3: 3.15)
Bicarbonate (HCO3)	numerical	meq/L	Median: 25.00 (Q1: 22.00, Q3: 28.00)
FiO2	numerical	fraction	Median: 0.40 (Q1: 0.40, Q3: 0.50)
Glucose	numerical	mg/dL	Median: 129.67 (Q1: 109.00, Q3: 157.60)
Blood Urea Nitrogen	numerical	mg/dL	Median: 24.00 (Q1: 15.00, Q3: 41.00)
Creatinine	numerical	mg/dL	Median: 1.00 (Q1: 0.70, Q3: 1.60)
Magnesium (Mg)	numerical	mg/dL	Median: 2.03 (Q1: 1.90, Q3: 2.27)
SGOT	numerical	u/L	Median: 41.00 (Q1: 25.00, Q3: 86.00)
SGPT	numerical	u/L	Median: 32.00 (Q1: 18.00, Q3: 69.00)
Total Bilirubin	numerical	mg/dL	Median: 0.70 (Q1: 0.40, Q3: 1.80)
White Blood Cell Count	numerical	E9/L	Median: 11.20 (Q1: 8.20, Q3: 15.20)
Platelets Count	numerical	E9/L	Median: 207.85 (Q1: 141.00, Q3: 296.00)
paO2	numerical	mmHg	Median: 105.25 (Q1: 82.57, Q3: 140.00)
paCO2	numerical	mmHg	Median: 40.22 (Q1: 35.25, Q3: 46.09)
Lactate	numerical	mmol/L	Median: 1.60 (Q1: 1.10, Q3: 2.30)
Total Input Fluids	numerical	mL	Median: 6569.08 (Q1: 2540.00, Q3: 13047.66)
Input 4H	numerical	mL	Median: 80.01 (Q1: 20.34, Q3: 327.50)
Max Vasopressors in 4H	numerical	mcg/kg/min	Median: 0.0002 (Q1: 0.00, Q3: 0.0017)
Total Volume Output	numerical	mL	Median: 3893.00 (Q1: 1300.00, Q3: 10070.00)
Output 4H	numerical	mL	Median: 248.00 (Q1: 105.00, Q3: 460.00)
Gender	binary	-	Male: 56.46% Female: 43.54%
Readmission of Patient	binary	-	False: 67.75% True: 32.25%
Mechanical Ventilation	binary	-	False: 46.89% True: 53.11%
Temperature (Temp)	categorical	Celsius	3 Classes <35.05: 8.64% 35.05-38: 79.65% >38: 11.71%
GCS	categorical	point	13 Classes 3: 5.10% 4: 0.76% 5: 0.93% 6: 4.51% 7: 3.72% 8: 4.12% 9: 5.17% 10: 7.93% 11: 9.68% 12: 3.98% 13: 3.45% 14: 13.03% 15: 37.61%
Pulse Oximetry Saturation	categorical	%	10 Classes [50.00,94.00]: 9.34% [94.00,95.29]: 10.54% [95.29,96.14]: 10.11% [96.14,96.80]: 9.49% [96.80,97.40]: 9.77% [97.40,98.00]: 8.70% [98.00,98.67]: 12.05% [98.67,99.25]: 9.96% [99.25,99.83]: 9.99% [99.83,100.00]: 10.05%
Partial Thromboplastin Time	categorical	s	10 Classes [0.00,24.50]: 9.69% [24.50,26.50]: 9.92% [26.50,28.10]: 10.35% [28.10,29.74]: 10.02% [29.74,31.70]: 9.76% [31.70,34.20]: 10.09% [34.20,37.60]: 10.08% [37.60,44.50]: 10.04% [44.50,60.90]: 10.04% [60.90,162.40]: 9.99%
Prothrombin Time	categorical	s	10 Classes [8.50,12.04]: 10.00% [12.04,12.90]: 9.77% [12.90,13.40]: 9.68% [13.40,13.80]: 9.67% [13.80,14.30]: 10.54% [14.30,14.90]: 10.03% [14.90,15.80]: 10.14% [15.80,17.40]: 9.99% [17.40,21.54]: 10.20% [21.54,193]: 9.98%
INR	categorical	-	10 Classes [0.10,1.04]: 10.00% [1.04,1.10]: 0.48% [1.10,1.19]: 17.55% [1.19,1.20]: 2.15% [1.20,1.30]: 16.88% [1.30,1.31]: 11.23% [1.31,1.46]: 11.68% [1.46,1.66]: 10.02% [1.66,2.2]: 9.79% [2.2,19.8]: 10.22%

Appendix C UMAP and t-SNE parameters

In this study, we used t-SNE and UMAP algorithms to perform dimensionality reduction on our datasets. The following parameters were used for each algorithm:

t-SNE:

Library: scikit-learn version 1.2.2

Parameters: $n_components = 2$, $n_iter = 400$, $perplexity = 40$

UMAP:

Library: umap-learn version 0.5.3

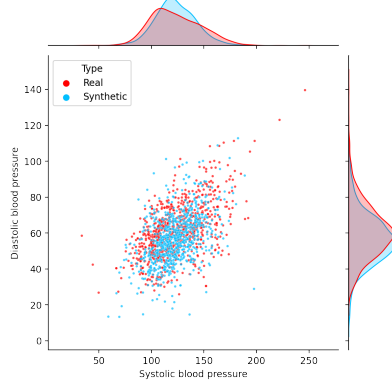
Parameters: $spread = 1$, $min_dist = 0.4$

Appendix D Joint distributions of variables

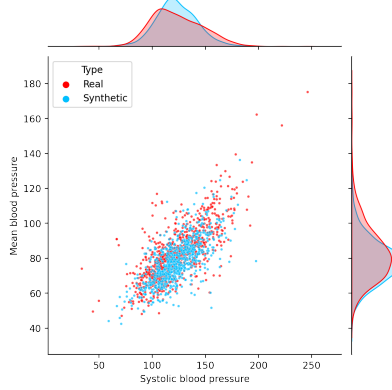
We have carried out an analysis of a set of variables that are clinically known to follow a joint distribution, namely systolic, diastolic and mean arterial blood pressure. This was to investigate whether CA-GAN can capture joint distributions of variables and whether synthetic data are clinically meaningful, where we know that systolic blood pressure is always higher than diastolic blood pressure. The results, shown using a scatter plot in Figure D4 show that the joint distribution of real data is similar to that of synthetic data.

Following from this, we have also implemented several sanity checks based on clinical knowledge to ensure that the generated synthetic data is clinically meaningful. In this respect, we have performed checks to investigate whether systolic BP values are always lower than diastolic. From our analysis, in the real sepsis dataset, 99.94% of values of these variables were correct; that is, systolic values were always lower than the diastolic values. In the synthetic sepsis dataset, this figure was 99.93%, with only 0.01% difference between the real and the synthetic dataset. On the other hand for the hypotension dataset there were 99.86% correct values of systolic and diastolic variables versus 99.84% in the synthetic dataset, representing a 0.02% difference. This analysis suggests that our architecture captures the structure of the real data quite well.

Systolic and Diastolic BP Joint Distribution



Systolic and Mean BP Joint Distribution



Mean and Diastolic BP Joint Distribution

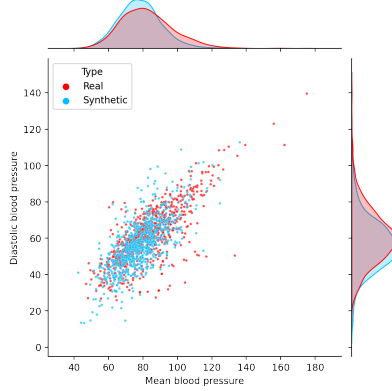


Fig. D4: Joint distribution plot of real sepsis data and CA-GAN synthetic data for the variables *Systolic blood pressure*, *Diastolic blood pressure* and *Mean arterial pressure*.

Appendix E Summary of distance metrics

Table E3: Statistics for KL-Divergence and Maximum Mean Discrepancy between the distribution of real and synthetic data.

	KL-divergence			MMD		
	SMOTE	WGAN-GP*	CA-GAN	SMOTE	WGAN-GP*	CA-GAN
MEDIAN	0.03407	0.02711	0.00629	0.00752	0.00217	0.00089
MEAN	0.05754	0.13518	0.14128	0.01500	0.05861	0.04790
STD DEV	0.07222	0.22330	0.31578	0.02385	0.09311	0.08457
MAX	0.28191	0.91622	1.36841	0.09954	0.25091	0.24806
MIN	0.00068	0.00010	0.00005	0.00047	0.00001	0.00001

(a) Acute hypotension data

	KL-divergence			MMD		
	SMOTE	WGAN-GP*	CA-GAN	SMOTE	WGAN-GP*	CA-GAN
MEDIAN	0.02296	0.06105	0.02292	0.00349	0.01299	0.00377
MEAN	0.09946	0.09282	0.06656	0.00583	0.03848	0.02505
STD DEV	0.29030	0.09704	0.08906	0.00702	0.13482	0.11603
MAX	1.88754	0.33564	0.39555	0.02948	0.90096	0.77536
MIN	0.00035	0.00240	0.00199	0.00002	0.00041	0.00003

(b) Sepsis data

Appendix F Description of Downstream Regression Task

For this task, the BiLSTM is trained on the first 20 hours for hypotension and 10 hours for sepsis of the patients' values to predict the next hour, using a sliding window approach. To ensure the fairness of our result, 15% of the time series data points of Black patients and a proportional representation of different genders were set apart as a test set. To account for the stochasticity of the models, we generated five synthetic datasets with CA-GAN. Then, we trained 5 BiLSTM models on each dataset for a total of 25 BiLSTM models (5x(5 per dataset)). The predictions of the trained models were then compared with the test dataset, and the resulting error was averaged across the five models and, subsequently, the five datasets.

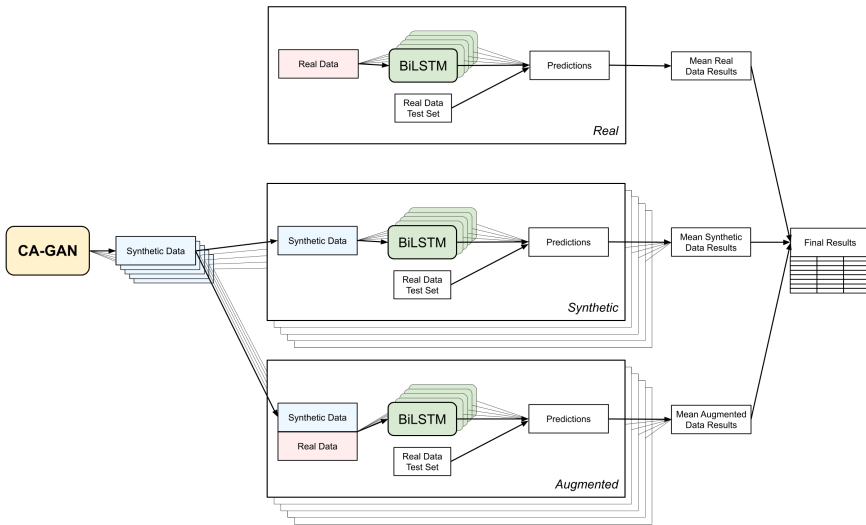


Fig. F5: Diagram of BiLSTM Model Training for Continuous Variable Prediction.

Appendix G Downstream regression task on gender-conditioned data

We have devised an additional dataset of patient subpopulations with gender as the underrepresented category. In this respect, we have created two datasets: one with the original data and the other (the surrogate dataset), where we have removed 80% of the data from female patients. We have replaced the removed portion of the dataset with the synthetic data generated from our architecture. Finally, we used a downstream regression task in the same manner as we used it with the ethnicity data to evaluate the performance of our approach.

Our results show that the performance of both algorithms is comparable, namely using the original dataset, we obtain a Mean Absolute Error (MAE) of 4.784 (± 0.393), while we obtain an MAE of 3.193 (± 0.052) using the synthetic dataset, indicating that the CA-GAN generates faithful synthetic data. What's even more interesting is that combining synthetic data with the real data further reduced the MAE to 2.870 (± 0.220), which is lower than that of the real data alone (MAE of 3.294 (± 0.241)).

	Real	Synthetic	Real Full	Augmented
Heart Rate	12.095 (0.190)	6.636 (0.536)	6.526 (0.330)	6.182 (0.250)
Systolic BP	21.662 (1.290)	10.803 (0.896)	11.453 (0.549)	9.909 (0.387)
Mean BP	10.280 (0.054)	6.342 (0.201)	7.055 (0.587)	6.507 (0.287)
Diastolic BP	9.308 (0.666)	6.304 (0.186)	7.029 (0.406)	6.131 (0.049)
Respiratory Rate	2.461 (0.071)	2.478 (0.196)	2.444 (0.065)	2.419 (0.107)
Potassium	0.258 (0.047)	0.195 (0.012)	0.158 (0.019)	0.190 (0.027)
Sodium	32.669 (1.528)	3.793 (0.149)	3.653 (0.071)	3.891 (0.204)
Chloride	10.612 (1.388)	4.013 (0.561)	5.013 (0.240)	3.700 (1.495)
Calcium	0.425 (0.030)	0.537 (0.129)	0.190 (0.060)	0.411 (0.091)
Ionised Ca	0.070 (0.015)	0.110 (0.032)	0.056 (0.004)	0.101 (0.043)
Carbon Dioxide	3.034 (0.820)	2.462 (0.155)	2.667 (0.744)	2.306 (0.112)
Albumin	0.514 (0.045)	0.458 (0.009)	0.474 (0.010)	0.460 (0.013)
Hemoglobin	0.729 (0.066)	0.677 (0.153)	0.596 (0.021)	0.666 (0.086)
pH	0.070 (0.020)	0.073 (0.044)	0.076 (0.038)	0.082 (0.019)
Arterial Base Excess	2.632 (0.098)	2.612 (0.037)	2.605 (0.078)	2.547 (0.032)
HCO3	3.278 (0.293)	2.651 (0.136)	3.172 (0.571)	2.490 (0.048)
FiO2	0.075 (0.015)	0.064 (0.003)	0.058 (0.003)	0.066 (0.005)
Glucose	46.868 (0.555)	28.239 (3.333)	24.431 (2.191)	26.405 (1.246)
Blood Urea Nitrogen	6.425 (0.814)	5.449 (0.414)	3.500 (0.979)	4.583 (0.329)
Creatinine	0.126 (0.025)	0.252 (0.076)	0.172 (0.107)	0.169 (0.022)
Magnesium	0.111 (0.015)	0.135 (0.041)	0.096 (0.021)	0.124 (0.028)
SGOT	130.591 (1.089)	127.034 (1.791)	136.685 (3.285)	126.824 (2.759)
SGPT	112.892 (2.177)	113.651 (5.488)	118.709 (3.904)	112.270 (3.293)
Total Bilirubin	1.552 (0.076)	1.347 (0.147)	1.552 (0.252)	1.398 (0.084)
WBC	0.990 (0.221)	1.280 (0.297)	1.101 (0.612)	1.195 (0.305)
Platelets Count	134.399 (4.411)	53.030 (3.271)	43.874 (4.875)	56.936 (5.577)
paO2	45.729 (0.515)	38.913 (0.811)	42.085 (1.316)	38.054 (1.368)
paCO2	6.954 (0.195)	5.867 (0.165)	6.866 (1.254)	5.861 (0.131)
Lactate	0.796 (0.048)	0.725 (0.015)	0.759 (0.025)	0.734 (0.020)
Input Fluids Total	10524.103 (9.990)	10136.382 (24.197)	10325.518 (27.476)	10086.376 (51.517)
Input 4H	158.433 (1.912)	137.386 (1.772)	154.167 (5.623)	138.082 (1.460)
Max Vasopressors 4H	0.065 (0.033)	0.036 (0.010)	0.026 (0.016)	0.033 (0.007)
Total Urine Output	10124.596 (5.131)	9774.791 (31.050)	9981.963 (13.985)	9759.179 (22.349)
Output 4H	210.089 (11.468)	159.417 (3.038)	163.217 (3.371)	158.430 (3.308)
Median	4.784 (0.393)	3.193 (0.052)	3.294 (0.241)	2.870 (0.220)

Table G4: Results of downstream regression task on gender-conditioned data, based on Mean Absolute Error (MAE), with standard deviation shown in brackets.